

MINIATURE CONFOCAL OPTICAL HEAD WITH INTEGRATED SCANNING  
AND CONFOCAL IMAGING SYSTEM USING SAID HEAD

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5 The present invention relates to a confocal optical head, in particular miniature, comprising integrated beam scanning means and a confocal imaging system equipped with said head.

10 More precisely, the present invention relates to an optical head and a corresponding optical system, in which a field to be imaged in a specimen is scanned point by point by an excitation signal. This type of system makes it possible to obtain, by means of data processing, a confocal image constructed point by point in real time. The confocal character is obtained by means of spatial filtering making it possible to detect a return signal originating solely from the excited point of the specimen taking the same optical path as the excitation signal.

15 One of the intended fields of application is that of high resolution confocal imaging, making it possible to observe and analyze a biological tissue *in vivo*, *in situ*, in real time, in particular accessible via the operating channel of an endoscope or integrated into the endoscope. The invention can also be applied to the fields of dermatology or gynaecology requiring less  
20 advanced miniaturization of the optical head. It can also be applied to the field of electronics for example for the control of semi-conductors or similar materials.

According to a first type of system, in particular described in the Patent Application WO 00/16151, an image guide is used, constituted by a bundle of  
25 flexible optical fibres, comprising at its distal end an optical focusing head intended to come into contact with the specimen to be analyzed. The excitation beam scanning means are situated at the proximal end of the image guide provided for scanning the fibres in turn. The confocal character resides here, in particular, in the fact that the same optical fibre of the guide is used to  
30 convey the excitation signal and the return signal emitted. This type of system has the advantage of an optical head simplified from the mechanical point of view and thus essentially comprising

optical focusing means which can be miniaturized. On the other hand, it has certain drawbacks, linked to the use of an array of optical fibres, in particular, the problem of sampling the tissue (continuity between the excitation points corresponding to the illumination of a fibre), the problem of injecting the fibres one by one and of the parasitic reflections at the inlet and outlet of the image guide, the sophisticated data processing of the image necessary in order to then correct the pattern of the fibres on the image, etc.

According to another known type of system, the beam scanning means are situated in the optical head at the distal end of an image guide comprising a single flexible optical fibre. The confocal character is obtained here due to the fact that the optical fibre is used for conveying the excitation signal and return signal emitted with an appropriate core diameter of the fibre.

The drawbacks of this type of system are then essentially linked to difficulties of miniaturizing the head, reproducibility and reliability of the mechanical means used for carrying out the scanning of the emergent beam of the optical fibre.

The document US 6,091,067 describes a scanning system in which an optical fibre is fixed to two bimorphic piezoelectric positioners, one of the positioners is placed in the axial direction of the fibre and the other in the direction perpendicular to the optical axis. The positioners, in order to offer an appropriate displacement relative to the field of view, must have a given length. Perpendicular to the axis of the optical fibre, this length constraint in fact leads to an optical head diameter too large for the *in vivo* applications *in situ* according to the present invention.

Several documents describe confocal miniature optical heads using micro-mechanical-type micro-mirrors (MEMs).

The Patent Application US 2002/0018276 describes a miniature confocal system using an optical fibre. The light leaving the fibre is reflected on the metallized part of a lens. This light is then reflected on a two-dimensional MEMs micro-mirror surrounding the fibre. The light is then sent towards the specimen via an optical system. The light returning from the specimen follows the reverse path and returns by the fibre which serves for spatial filtering. The system is miniature, being 2 mm in diameter and 2.5 mm in length.

The patents US 6,154,305, US 6,088,145, US 6,007,208, US 5,907,425 and US 5,742,419, describe a confocal head in which the scanning of the field of view is carried out by two electrostatically pivoted MEMs micro-mirrors. The proposed head can be miniaturized but on the other hand offers a 60 x 60  $\mu\text{m}$  field of view which is too small with respect to the applications according to the invention corresponding to a field measuring 100 x 100  $\mu\text{m}$  minimum in order to be able to observe, for example, several nuclei which are 5  $\mu\text{m}$  in diameter generally spaced out at intervals of several tens of  $\mu\text{m}$ . The number of images per second of 5 to 8 is moreover also insufficient for imagery in real time (requiring a minimum of 10 to 12 images per second in the slowest mode with 640 lines). Moreover also, the field of view is situated parallel to the axis of the optical fibre, which can lead to practical difficulties of use (correct positioning of the probe).

The patents US 6,172,789 and US 6,057,952 describe a confocal optical head with a field of view this time in the axis of the optical fibre and allowing adjustment of the depth of the observation plane. The scanning means include a mobile mirror and a fixed mirror. The mobile mirror has an opening in its centre, and is of MEMs type, mounted so as to be able to pivot at least in one direction. The reflection surfaces of the mobile and fixed mirrors are situated face-to-face. The light leaving the optical fibre passes through the opening in the mobile mirror, then is reflected by the fixed mirror in the direction of the mobile mirror.

The following drawbacks in particular are encountered with such a head construction: significant cost of the mobile mirror with a hole in the centre, and also the scanning speed of such a two-dimensional MEMs mirror which is not sufficient for imagery in real time.

- 5        Generally, the change in direction of the optical beam by successive reflections on micro-mirrors leads to optical faults which are complicated to correct, in particular distortion or field curvature.

10        The purpose of the present invention is to overcome these drawbacks and propose an optical head which is of high resolution, confocal (offering an axial optical resolution of approximately 1 to 2  $\mu\text{m}$ ) and which comprises scanning means integrated with an excitation beam. According to other objectives, the optical head must be able to be miniaturized (not exceeding 3 mm in diameter in total), to make it possible to produce an image in real time (at least 10 images/second) and to cover a field to be imaged of the order of  
15        100 x 100  $\mu\text{m}$  minimum and preferably 150 x 150  $\mu\text{m}$ .

It proposes a miniature confocal optical head for a confocal imaging system, in particular endoscopic, said head comprising:

- a point source producing an excitation beam;
  - optical means capable, in particular, of causing said optical beam to  
20        converge into an excitation point situated in a subsurface plane relative to the surface of a specimen, said plane being perpendicular to the optical axis of the optical head; and
  - means of scanning said excitation point so as to describe a field of view in said subsurface plane in two perpendicular scanning directions, rapid line  
25        scanning and slow column scanning,
- characterized by MEMs mechanical micro-system means capable of moving in translation according to a chosen displacement at least one of the optical means which is mobile in a direction perpendicular to said optical axis so as to obtain at least one of said scanning directions.

According to the invention, lateral beam scanning is carried out by moving laterally relative to the optical axis one of the transmission optics, the optical axis of the optical head is thus modified only laterally and non-  
5 angularly as with reflection optics. This has the advantages of preserving an axial illumination of the specimen and minimizing the diameter of the optical head.

The mechanical micro-system means belong to the family of micro-components, known by the generic name of MEMs, making it possible to carry  
10 out scanning operations, switches, deflections (in particular of mirrors) etc., actuated by the pulse generally of an electric field.

The MEMs means which can be used according to the invention are in particular the following:

- electrostatic actuators using the attractive force between two charges;
- 15 - thermal actuators using a temperature gradient or the difference in thermal dilatation coefficient between two materials, an electric current creating for example a rise in temperature;
- magnetic actuators using the force resulting from the interaction of two magnetic fields; generally, a field external and a field internal to the MEMs  
20 are applied, for example a coil creating an external field when an electric current passes through it.

The MEMs have a response time compatible with the movement of an optical means, in particular a lens, over a distance, allowing for magnification, corresponding to the dimension of the field to be imaged according to the  
25 invention, namely of the order of 150  $\mu\text{m}$ , and at a speed allowing a choice of slow scanning comprised between approximately 10 and 15 Hz, corresponding to column scanning of the field to be imaged, or rapid scanning of approximately 4 kHz, corresponding to line scanning of the field. The MEMs moreover have dimensions compatible with a miniaturization of the optical  
30 head, of the order of 2 to 3 mm in total diameter, as shown by the detailed description given hereafter. They make it possible to impart a

stable and repeatable movement of the optics. Preferably, to this end, the MEMs means used according to the invention are constituted by means of movement, for example pairs of electrostatic combs, arranged in a diametrically opposite manner and actuated according to different modes, simultaneously or alternately. Other MEMs systems also exist in the form of a ring in the opening of which a lens can be fixed and also operating alternately in order to impart a reciprocating translation movement.

The point source can be of fibre type, and therefore offset: the end of a flexible optical fibre connected to a laser source is fixed to the optical head. The source can also be constituted by a VCSEL (Vertical-Cavity Semiconductor Emitting Laser) component which is virtually a point laser source having a cavity the outlet of which measures a few microns in diameter. In both cases, the dimension of the source (core diameter of the optical fibre or diameter of the outlet of the cavity of the VCSEL component) is chosen in order to be able to serve as a filtering hole of the backscattered signal and to produce a confocal image. If a VCSEL source is used, a detector is placed just behind the cavity in order to construct the detection route. Moreover, the numerical aperture of the source, fibre type or VCSEL type, is chosen in order to collect the maximum amount of photons emitted by each excitation spot, typically comprised between 0.2 and 0.4.

The optical means used in the optical head generally comprise first optical means, placed at a chosen focal distance from the point source, capable of transforming the excitation beam emitted from the source, which is divergent because of the numerical aperture of the source, to a parallel or slightly divergent beam. These optical means are constituted by a lens or by a set of refractive (standard or with an index gradient) and/or diffractive lenses. Diffractive lenses have the advantage of being smaller and lighter. Second optical means placed at a chosen focal distance from the first optical means then have the function of focusing the optical beam into an excitation point

situated in the subsurface observation plane. These optical means can also be constituted by a lens or by a set of refractive and/or diffractive lenses.

Preferably, MEMs means are utilized according to the invention for displacing the first optical means rather than the second optical means and at a frequency making it possible to carry out slow column scanning. The scanning of the second optical means would lead to additional optical aberrations because of their large numerical aperture on the specimen.

As regards rapid line scanning, according to the invention, the latter can be carried out either by moving the source, using for example suitable piezoelectric means, or with a fixed source and movement of the second optical means also using appropriate MEMs means and in a direction perpendicular to the movement of the first optical means.

Additional scanning in the z direction, in order to modify the depth of visualization, can moreover be provided in the optical head according to the invention, for example using MEMs means capable of moving the mobile optical means along the optical axis of the optical head, or using means capable of modifying the radius of curvature of one of the optical means, preferably that closest to the specimen. Such scanning advantageously makes it possible to re-create a 3D image by data processing.

The present invention also proposes a confocal imaging system using an optical head as defined above. According to a first example, the system comprises a fibre-type source. According to a second example, it comprises a VCSEL-type source associated with detection means integrated in the optical head and flexible linking means between said head and the signal data processing means.

The present invention will be better understood and other advantages will appear more clearly in light of the following description

of embodiments, a description made with reference to the attached drawings in which:

- Figure 1 is a general diagram of an example of a fibre-type confocal imaging system using the miniature head according to the invention;
- 5    - Figure 2 is a side cross-section of a miniature head according to a first embodiment;
- Figure 3 is an optical diagram of the miniature head of Figure 2; and
- Figure 4 is a view similar to Figure 2 illustrating a second possible embodiment.

10    Figure 1 schematically represents a fibre-type confocal imaging system which can include a miniature head according to the invention.

The system comprises a source 1, for example a laser source, capable of emitting an excitation signal with a wavelength capable of generating in a specimen a return fluorescence or backscattering signal, said signal being  
15    conveyed by a first single-mode optical fibre 2a to coupling means 3, for example a 50/50 fibre coupler, provided in order to direct the excitation signal originating from the source 1 into a single-mode optical fibre 2b at the end of which the miniature optical head 4 according to the invention is situated and in order to direct the return signal originating from the excited site towards  
20    detection means 5, for example a photodetector, using a third single-mode optical fibre 2c. The system comprises electronic control, command and synchronization means 6, making it possible to control the source 1, the scanning means of the optical head 4 and the detection means 5, in a synchronized manner, in order in particular to know the location of the signal  
25    in the specimen in order to allow the construction of an image in real time. The system moreover comprises electronic means 7, of amplification, forming and A/D conversion of the signal detected by the detection means



5, data-processing means 8 comprising an acquisition card and a graphics card and means of displaying 9 the images obtained.

This system operates overall in the following manner: the miniature optical head 4 is brought into contact with a specimen to be analyzed, for example via the operating channel of an endoscope. The source 1 sends an excitation signal with a chosen wavelength into the portion of fibre 2a. The coupler 3 directs the excitation signal into the portion of fibre 2b guiding the signal into the optical head 4 where it is scanned and focused on an analysis surface (or analysis field) in a plane of the specimen perpendicular to the optical axis defined by the optical fibre 2b, at a given depth in the specimen. A return signal originating from the scanned surface in the specimen follows the reverse path of the excitation signal as far as the coupler 3: it is picked up by the optical means of the optical head 4, recoupled in the portion of fibre 2b, then directed by the coupler 3 into the portion of fibre 2c towards the detector 5. The signal detected is amplified and converted to a digital signal, then subjected to data-processing in order to finally constitute an image element displayed in real time.

The miniature head according to the invention is now described in detail with reference to the chosen embodiment and represented in Figure 2.

The head comprises, in a mechanical support structure 15:

- piezoelectric-type means 11 to which is fixed the terminal portion of the optical fibre 2b, capable of moving this terminal part of optical fibre, and therefore the optical beam leaving the latter, approximately in reciprocating translation along a chosen displacement  $D_L$ , approximately perpendicular to the optical axis A defined by the optical fibre, and corresponding to a displacement on a line of the field to be imaged (these piezoelectric means are described hereafter in detail);

- first optical means 12 capable of converting the beam leaving the fibre 2b which is diverged to a parallel or slightly divergent beam, and picking up the return beam originating from the specimen; these optical means are according to the invention mobile in translation, so as to move

the optical beam along a chosen displacement, schematically shown by the double arrow, perpendicular to the displacement  $D_L$ , and corresponding to a column displacement of the field to be imaged;

- MEMs-type micro-mechanical means, 14a and 14b, capable of reciprocally moving the optical means 12 along the displacement  $D_L$  (these means are described hereafter in detail);
- second fixed optical means 13 capable of causing said parallel beam to converge in order to focus it into a point or spot S in a plane P of the examined specimen E situated at a given depth and approximately perpendicular to the optical axis A.

The piezoelectric means 11 and the MEMs means 14a and 14b thus together make it possible to carry out the scanning of the beam focused on the field to be imaged, the piezoelectric means 11 serving to carry out a rapid line scanning and the MEMs means 14a and 14b serving to carry out slow column scanning.

The mechanical support structure 15 is constituted by a hollow body 16, for example a tubular optic holder, with, at one end, a tight window 17, intended to come into contact with the specimen E, capable of being passes through by the excitation and return backscattering or fluorescence signals, and with, at its other end, a passage 18 for the terminal portion of the optical fibre 2b and also for the piezoelectric means 11. A side wall 19 surrounds the passage 18 in order to tightly seal the optical head. The fixed optical means 13 are fixed and centred relative to the optical axis A inside the body 16, and the mobile optical means 12 are linked to the inside face of the body 16 via the MEMs means 14a and 14b as explained hereafter in detail.

The optical fibre 2b coupled to the optical head is preferably single-mode, allowing the most homogeneous possible illumination of the specimen. The numerical aperture of the fibre is chosen to be as large as possible in order to allow an optimized collection of photons, and in order to allow, together with an appropriate core diameter, a coupling

of the return signal in the fibre, and therefore spatial filtering, which is the best possible. Typically, the numerical aperture is 0.4 and the core diameter comprised between 1 and 2  $\mu\text{m}$ . This choice of characteristics for the optical fibre, together with the characteristics of the optical means 12 and 13, make it possible to carry out spatial filtering of the return signal ensuring the confocality of the system.

According to the example chosen, the piezoelectric means 11 are constituted by a piezoelectric positioner having a surface on which is fixed, for example by gluing, the terminal part of the optical fibre 2b with an end portion of the protruding fibre. This positioner 11 is double, therefore called bimorphic, having the feature of being deformed when an electrical voltage is applied to it; this makes it possible to move the optical fibre between a non-excited or rest position of the positioner and an excited position corresponding to the excitation of the positioner. The positioner 11 is chosen so as to exhibit a displacement between these two positions, allowing for magnification, corresponding to the field width which is to be imaged in the specimen. Moreover, positioner 11 is chosen so as to be able to be excited at a frequency making it possible to carry out the desired rapid line scanning of the specimen. Moreover, for a positioner of given length, compatible at its maximum with miniaturization, a maximum scanning amplitude can be obtained by exciting the positioner at its resonant frequency. Typically, a positioner of 7.5 mm in length, excited with a sinusoidal excitation voltage of  $\pm 60\text{V}$ , makes it possible to achieve a resonant frequency of 4 kHz, making it possible to carry out line scanning at a speed appropriate to imaging in real time (at least 10 images/second), over a imaged field 150  $\mu\text{m}$  in width (with unitary magnification). This length is compatible with the maximum total dimension for the head of approximately 30 mm. The width of the positioner (dimension perpendicular to the optical fibre) influences neither the resonance, nor the amplitude of scanning. Typically, the width of the positioner can be a few hundred microns, not exceeding the outside maximum total diameter provided for the

head, approximately from 2 to 3 mm. In order to take account of a magnification greater than 1, for a given imaged field dimension, a longer piezoelectric positioner can be chosen in order to have a greater displacement and possessing a higher excitation voltage ( $\pm 100V$  to  $120V$ ). The system  
5 moreover comprises the safety means necessary for the use of electrical voltages of this order for *in vivo* applications.

The MEMs means 14a and 14b serve to laterally move the mobile optical means 12 in a direction perpendicular to that of the movement of the fibre imparted by the piezoelectric means. More particularly according to the  
10 example chosen and represented in the figures, the mobile optical means 12 being constituted by a single lens, the MEMs means include two pairs of combs 14a and 14b, diametrically opposite, each pair of combs comprises one comb fixed to said lens 12 and one comb assembled with the body 16. The combs are semi-conductor filaments which are aligned and the two  
15 combs in a pair have their filaments overlapping. The movement of the lens 12 is obtained by shifting one comb relative to the other by means of an electrostatic effect. The transversal movement achieved by means of the pairs of combs is perpendicular to the axis of the fibre. It is carried out at a slow frequency (typically from 10 to 15 Hz) and makes it possible to produce an  
20 imaged field size of  $150\text{ }\mu\text{m}$  by choosing the appropriate scanning amplitude.

The mobile optical means 12 has the function of transforming the emergent divergent beam from the optical fibre 2b into a parallel or divergent beam. It must correspond to dimension constraints: its diameter must be compatible with a miniaturization of the head which must have a total external  
25 diameter of 2 to 3 mm maximum. It must correspond to mechanical constraints and be sufficiently solid and resistant to be able to be integral with the MEMs means 14 and actuated in translation. It must also correspond to optical constraints: its diameter must be sufficiently large relative to the diameter of the beam projected for the

imaged field that is to be obtained (otherwise there is a risk of observing faults at the field edge (in particular vignetting)); the numerical aperture of the optical means 12 must be at least equal to or preferably greater than the numerical aperture of the fibre in order to preserve the confocality of the head and optimization of the number of photons detected during scanning. A minimum optical diameter of 1 mm can be obtained with a numerical aperture greater than 0.4 (numerical aperture of the optical fibre 2b), which is compatible with a miniature head 2 to 3 mm in outer diameter and the insertion of the MEMs means 14. By way of example, according to the most simplified mode, this optical means 12 is a standard lens but could also be a doublet of lenses or any other usual optical means making it possible to preserve a size and weight compatible with the sought objectives. As an example of more sophisticated optics, a diffractive lens can be used using diffraction in order to decompose the wave front of the incident beam on different zones and which after recombination makes it possible to obtain the sought wave front. Moreover, these optics have the advantages of a large numerical aperture, a small space requirement, low weight and low cost.

The fixed optical means 13 must make it possible to focus the scanned beam onto a spot S at a certain depth in the specimen in a focusing plane and to collect a maximum amount of photons originating from each spot in this same focusing plane. The characteristics of these optical means (in particular the magnification and the numerical aperture) are defined taking account of the specifications of the optical fibre and mobile optical means 12 in order to ensure confocality for the whole of the system and also in order to minimize the optical aberrations which could be engendered by the scanning (distortion, instability, shifting of the mobile optical means with respect to the optical axis etc.).

The exit window 17 is the last interface situated between the optical head and the specimen. It has the function of protecting the optics, and

also of carrying out an index matching between the head and the specimen, in particular by means of a treatment of its external face for example for an index of 1.33 equal to that of water. The window can as a variant also be constituted by a lens having a refractive power function on the optical beam.

5        Figure 3 shows an optical diagram of the head which has just been described according to a possible particular example, illustrating in particular the line scanning of the specimen, on which the fibre 2b is represented in a standard fashion in its rest position I and in two extreme lateral positions II and III.

10        The optical specifications are the following:

- scanned field:  $2\Delta x = 400 \mu\text{m}$
- core diameter of the fibre 2b:  $\varnothing_{\text{core}} = 1.3 \mu\text{m}$
- numerical aperture of the fibre 2b: numerical aperture =  $\sin(\alpha_1) = 0.4$
- lens 12: diffractive
- 15        - focal length of the mobile lens 12:  $f_{12} = 1.83 \text{ mm}$
- total diameter of the lens 12:  $\varnothing_{12} = 2 \text{ mm}$
- lens 13: diffractive
- focal length of the fixed lens 13:  $f_{13} = 0.73 \text{ mm}$
- total diameter of lens 13:  $\varnothing_{13} = 1.6 \text{ mm}$
- 20        - magnification of the optical system =  $G = 2.5$
- imaged field =  $2\Delta x \text{ object} = 160 \mu\text{m}$
- numerical aperture object = numerical aperture object =  $n \sin(\alpha_2) = 1$  (in water  $n = 1.33$ )
- diameter of each spot S focused in the specimen: limited by diffraction
- 25        over the whole imaged field.

In the example which has just been described, the rapid line scanning means of the excitation spot are produced using a piezoelectric positioner to which the end of the optical fibre is fixed. According to a

possible embodiment variant, the optical fibre is fixed and the lens 13 is mobile, MEMs means, similar to the means 14a and 14b, being used in order to move the optical lens 13 in a direction perpendicular to the movement of translation of the mobile optical means 12 and according to a frequency compatible with rapid line scanning (4 KHz). Also as a variant, conversely, rapid scanning can be carried out by moving the lens 12 and slow scanning by moving the lens 13.

Figure 4 also shows an embodiment variant of the optical head of Figure 2, the identical means having the same references as in Figure 2. In this variant, means 16a and 16b, fixed on one side to the tubular optic holder 15 and on the other to the lens 13, are used to move said lens 13 along the optical axis A of the head, making it possible to adjust the depth of visualization in the specimen, approximately over a few tens of  $\mu\text{m}$ , schematically shown by the double arrow Z. This advantageously makes it possible to produce three-dimensional reconstructions of the specimen which is observed: different two-dimensional data acquisitions are made at different depths and it is then possible to reconstruct the observed volume by data processing. In other cases, the adjustment of the depth of visualization can make it possible to advantageously adapt to the specimen observed, at the optimum depth of visualization of the specimen. The movement of the optical means 13 in the axial direction of the head makes it possible to cause the beam to converge at a different distance. The means 16a, 16b are of MEMs or piezoelectric type.

Also as an embodiment variant, the optical head can comprise instead of the optical fibre 2b a VCSEL-type point source associated with a detector placed just behind the cavity of the VCSEL. By way of example, with reference to Figure 3, the following optical specifications can be given:

- field scanned:  $2\Delta x = 400\text{-}600 \mu\text{m}$
- diameter of the opening of the VCSEL cavity:  $\varnothing_{\text{cavity}} = 2\text{-}4 \mu\text{m}$

- numerical aperture of the VCSEL cavity: numerical aperture =  $\sin(\alpha_1) = 0.25$  (in air)
- lens 12: diffractive
- 5 - focal length of the mobile lens 12:  $f_{12} = 3 \text{ mm}$
- total diameter of the lens 12:  $\varnothing_{12} = 2 \text{ mm}$
- lens 13: diffractive
- focal length of the fixed lens 13:  $f_{13} = 1.17 \text{ mm}$
- total diameter of lens 13:  $\varnothing_{13} = 1.6 \text{ mm}$
- 10 - magnification of the optical system =  $G = 3$
- imaged field =  $2\Delta x_{\text{object}} = 160 - 240 \mu\text{m}$
- numerical aperture object =  $\text{NA}_{\text{object}} = n \sin(\alpha_2) = 0.75$  (in water  $n = 1.33$ )
- diameter of each spot S focused in the specimen: limited by diffraction
- 15 over the whole imaged field.